Palestine Polytechnic University



College of engineering & technology Computer & electrical engineering department

Graduation project

Electrical Sleep Inducer

Prepared by: Alla` A. Shabaneh

Project supervisor Dr. Ramzi Al-Qawasmi

Hebron – Palestine

June – 2011

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This report is submitted in partial fulfillment of the requirements for the degree of B.Sc. in biomedical engineering

> Project supervisor Dr. Ramzi Al-Qawasmi



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June – 2011

جامعة بوليتكنك فلسطين

الخليل _ فلسطين

كلية الهندسة والتكنولوجيا

دائرة الهندسة الكهربائية والحاسوب

محفز النوم الكهربائي (جهاز النوم)

آلاء عبد العزيز شبانة

بناء على نظام كلية الهندسة والتكنولوجيا وإشراف ومتابعة المشرف المباشر اللجنة الممتحنة تم تقديم هذا المشروع إلى دائرة الهندسة الكهربائية والحاسوب وذلك استكمالا لمتطلبات درجة البكالوريوس في الهندسة تخصص الاجهزة الطبية.

توقيع المشرف

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توقيع اللجنة

توقيع رئيس الدائرة

إليك جديّ الحبيبة. لتي عانت ولفترة طويلة من الأرق ... ومعاناتها هي التي دفعتني إلى اختيار هذا الموضوع دون سواه ليكون مشروعي للتخرج ... علَني استطيع مساعدةها ومساعدة غيرها على التغلب على هذا المرض

إليك والدي الحبيب . . من يضيع غراسك الذي غرسته في نفسي وسأظل دوماً ابنتك التي تفخر بما ولن أخيب ظنك بإذن الله

اليك أمى .

ن للجنة دروبا أنت خطاها .. وللنار حجابا أنت ستائره .. ران للنجاح سلما رضاك درجاته وللغضب أودية غضبك دلالاته .. فمنّي علي بخطا الجنة .. وأكرميني بستائر النار وتفضلي عليّ بدرجات النجاح والتوفيق على الرغم من تقصيري Acknowledgment

First all prais is to allah who gave me the ability to complete this project with a satisfing degree of perfection

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Thanks to palestine polytechnic university *L* every body shared to success my project.

Abstract

Sleeping difficulty, called insomnia, can involve difficulty falling asleep when you first go to bed at night, waking up too early in the morning, and waking up often during the night.

The lack of restful sleep can affect your ability to carry out daily responsibilities because you are too tired or have trouble concentrating. All types of insomnia can lead to daytime drowsiness, poor concentration, tension and nervousness and the inability to feel refreshed and rested in the morning.

Many people experience sleeping well in natural surroundings, into a tent or a wooden hut. This fact is due not only to the healthy atmosphere but also from our unconscious ability to perceive natural Earth's magnetic fields.

Magnetic field associated with the Earth is called Geo-magnetic fields. It is essentially dipolar (i.e., it has two poles, the northern and southern magnetic poles) on the Earth's surface. Away from the surface, the field becomes distorted.

My project generates this type of Geo-magnetic-fields and the basic aim is to perceive them: in this manner our brain is surrounded by an ideal environment for a sound sleep. And it is also helpful

The goal of this project is to implement a device that generates magnetic fields that is similar to Geo-magnetic fields using preset durations depending on the patient's case.

صعوبة الخلود الى النوم او هروب النوم يدعى الأرق الذي ينطوي على استعصاء النوم عند الذهاب الى الفراش وتقطعه وانخفاض جودته وبالتالي صعوبة الاستيقاظ صباحاً.

عدم التمتع بنوم مريح يؤثر سلباً على النشاطات اليومية بسبب التعب وصعوبة التركيز. جميع أنواع الأرق الإغفاء و النعاس بالنهار وقلة التركيز وعدم الشعور بالنشاط خلال النهار والشعور بالتوتر والعصبية يؤثر على الشخص في عمله ومجريات سير يومه

العديد من الناس تتمتع بنوم جيد في الطبيعة. و هذة الحقيقة ليست نتيجة فقط للجو الصحي وإنما لزيادة القدرة على استقبال الحقول المغناطيسية الطبيعية المنبعثة من الأرض والتأثر بها.و هذة المجالات المغناطيسية يكون تأثير ها اقوى كلما اق

> في هذا المشروع يقوم الجهاز بتوليد هذه المجالات المغناطيسية وبذلك يحيط الدماغ بالجو () ولا يفيد فقط بالمساعدة على النوم بل ويساعد ايضا في تهدئة الأعصاب.

والهدف من هذا المشروع تطبيق جهاز يمكنه توليد مجالات مغناطيسية مشابهه للمجالات المغناطيسية الأرضية ولفترات زمنية مختلفة حسب حالة المريض وحاجته.

Glossary

CES Cranial electrotherapy stimulation

Thalamus The area of the brain that relays sensory information to the cerebral cortex.

Sleep paralysis The temporary inability to talk or move when falling asleep or waking up. It occurs normally during REM sleep.

Sleep hygiene The collection of behaviors and environmental conditions that influence the length and quality of sleep

Pons The brainstem region critical for initiating REM sleep

Electroencephalogram (EEG) A measurement of the electrical activity associated with brain activity.

Electromyograms (EMG) A measurement of the electrical activity associated with muscle movements.

Electrooculogram (EOG) A measurement of the electrical activity associated with eye movements.

Cerebral cortex The brain's outer layer of gray tissue that is responsible for higher nervous function.

Hypnogram A graphical summary of the electrical activities occurring during a night's sleep

Insomnia Sleeplessness; chronic difficulty with sleep onset or maintenance of sleep, or a perception of nonrefreshing sleep.

Sleep hygiene The collection of behaviors and environmental conditions that influence the length and quality of sleep.

The scalp The anatomical area bordered by the face interiorly and the neck to the sides and posterior.

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CHAPTER 1

Introduction

- 1.1 Overview
- **1.2 Project Objectives**
- **1.3 Literature Review**
- **1.4 The Importance of the Project**
- 1.5 Time plan
- **1.6 Project cost**
- **1.7 Project contents**

1.1.Overview

This project is aimed to design and build a simple device which generates magnetic field similar to geo-magnetic field, the device consists of oscillator to generate square wave signal to drive counter and timer, a radiator coil to generate electromagnetic field and timer to set desired time duration.

The objectives can be summarized as follow:

- 1- design and build a system which generates geo-magnetic field
- 2- use different time durations
- 3- select between two modes



Fig1.1: General Geomagnetic generator block diagram

1.2.project objectives

The main objectives are:

- 1. to Generate a natural electromagnetic-field
- 2. Induces a prolonged and sound sleep without drugs
- 3. to study the physiology of sleep and brain waves (EEG)
- 4. design and implement a device for generating the desired field with several durations and two modes of operation
- 5. helping the chronic insomnia patients to enhance their sleeping habits

1.3.literature review

Insomnia is a disorder that can make it hard to fall asleep, hard to stay asleep, or both. With insomnia, you usually awaken feeling unrefreshed, which takes a toll on your ability to function during the day. Insomnia can sap not only your energy level and mood but also your health, work performance and quality of life.

How much sleep is enough varies from person to person. Most adults need seven to eight hours a night. Many adults experience insomnia at some point, but some people have long-term (chronic) insomnia.

a) During the first half of the twentieth century many different methods were used in clinical settings to put patients to sleep Drs. Leduc and Rouxeau of France were the first to experiment with low intensity electrical stimulation of the brain in 1902.

Initially, this method was called electro sleep as brain stimulation was considered a sleep inducer. There were other names such as transcranial electrotherapy (TCET) and neuroelectric therapy (NET), but research on CES began in the Soviet Union during the 1950s and was introduced in the US about a decade later (Iwanovsky & Dodge, 1968).

- b) Electroconvulsive therapy (ECT) for depression, lake of sleep (insomnia) and psychosis was introduced in 1933 by Cerletti and Bibi (1938). ECT typically involved the application of 120 volts with 500 milliamperes at 60 Hz for 0.2 seconds. ECT caused convulsions and a loss of consciousness rather than sleep, for a limited time. Subsequently, the electrical current was reduced to around 30 milliamperes, using 2 volts at 700 Hz. This less intense form of transcranial stimulation was called electroanaesthesia (National Research Council, 1974). Patients remained asleep as long as the current was on, but tended to wake up immediately when the current was turned off
- c) Nerve Excitation Models: The introduction of nerve excitation models has widened our understanding of the mechanisms of nerve excitation elicited by magnetic stimulation [Basser and Roth, 1991; Esselle and Stuchly, 1992; Nagarajan and Durand, 1993; Hyodo and Ueno, 1996]. The theoretical nerve excitation models have shown that for neuronal excitation, a negative peak of the spatial gradient of induced electric fields, the activating function, contributes to the depolarization of the membrane. The site of neuronal excitation corresponds to the site of the maximal value of the activating function.

1.4.The importance of the project:

This device helps fighting insomnia. Apart from this it is support relaxation, stress management and induce sleep easily.

- Generates a natural electromagnetic-field
- Simple to use and safe
- Non invasive method
- Make it easier to fall asleep
- Induces a prolonged and sound sleep without drugs
- No side effects

1.5.Time plan

Table 1.1: project time

Week	1	2	3	4	5	6	7	6	9	10	11	12	13	14	15	16
Give ideas																
Data																
collection																
Making																
circuit																
Analysis																
Writing																
Presentation																

1.6. Project Cost:

Item	# of Pisces	Price (NIS)
4060 ripple counter and oscillator	1	8
4093 quad 2 input Schmitt NAND gate	1	7
Diodes (IN4148)	4	2
Switches	4	16
Push button	1	3
Battery PP3 9V	1	9
Resistors (different values)	9	3
PNP transistor (BC327)	1	3
Radiator coil	1	5
Capacitor 47µF	2	2
Capacitor 100nF	1	1
Capacitor 330nF	2	3
Capacitor 15nF	2	3
TOTAL		64

Table 1.2: project cost

1.7.Project content

Chapter one: Introduction Chapter two: physiological background Chapter three: project circuit Chapter four: conclusions and future work

CHAPTER 2

Physiological Background

2.1 Introduction

- 2.2 Sleep
 - 2.2.1 Sleep is a dynamic process
 - 2.2.2 Physiological changes during sleep
 - 2.2.3 Sleep and the brain
 - 2.2.4 Sleep Patterns
 - **2.2.5 Sleep Disorders**
 - 2.2.6 Insomnia
- **2.3 EEG**
- 2.4 Geomagnetic Field

2.1 Introduction

There is nothing quite as great as being able to sleep soundly all night long. After a sound sleep the world just seems a little brighter because the importance of a sound sleep to health is the repair of cells in the body as well as forming memories. A sound sleep is often referred to as 'getting your beauty sleep' which is technically true.

Deep sleep literally regulates the body health in adults, the Human Growth Hormone balance, and the skin which is actually the largest organ of the body and also growth in children. Proper sleep patterns are also important for maintaining the immune system of the body and for improving the powers of concentration.

Going without proper sleep happens for a number of reasons. It can be related to overall health levels, stress, anxiety, noise or irregular lifestyle patterns. Whatever the reason there are a number of ways to try to correct sleep patterns including massage therapy and prescription drugs. These may or may not be effective or even safe curatives but the electrical Sleep Inducer offers a health aid that is safe, easy to use and effective in regulating sleep patterns...

2.2 Sleep

Sleep is essential to survival. When we sleep our bodies are restored and healed, memories are built and damaged cells are repaired. Healthy sleeping habits can also improve hormone and immune system functions.

Sleep deprivation can lead to hypertension, emotional and physical stress, depression and obesity, not to mention inability to concentrate and poor performance on work tasks. While there are a number of treatments to regulate sleep, such as massage therapies and sleeping pills, the electrical Sleep Inducer can help you to fall asleep without having to take drugs or drive to see a massage therapist.

Sleep is often thought to help conserve energy, but actually decreases metabolism only about 5–10%, Sleep is generally divided into 2 broad types: nonrapid eye movement (NREM) sleep and REM sleep. Based on EEG changes, NREM is divided further into 4 stages (stage I, stage II, stage III, stage IV).

Very few textbooks for high school students provide any scientific information about changes that occur in the body during sleep and how those changes affect our ability to move and think. Of course, we've heard that a good night's sleep will help us perform better on a test the next day, but is this based on scientific fact, or is it just a continuing myth? The lack of information in textbooks may be due to the fact that sleep research is only recently gaining recognition. A great deal remains to be learned through scientific studies, including an answer to the key question, What is the function of sleep? Although its function remains unclear, research is providing a great deal of information about what happens in the brain and body during sleep and how the body regulates sleep.

The purposes and mechanisms of sleep are only partially clear and are the subject of intense research.

2.2.1 Sleep is a dynamic process

Sleep is not a passive event, but rather an active process involving characteristic physiological changes in the organs of the body. Scientists study sleep by measuring the electrical changes in the brain using **electroencephalograms (EEGs)**. Typically, electrodes are placed on the scalp in a symmetrical pattern. The electrodes measure very small voltages that scientists think are caused by synchronized activity in very large numbers of synapses (nerve connections) in the brain's outer layers (cerebral cortex). EEG data are represented by curves that are classified according to their frequencies. The wavy lines of the EEG are called brain waves.

An electrooculogram (EOG) uses electrodes on the skin near the eye to measure changes in voltage as the eye rotates in its socket. Scientists also measure the electrical activity associated with active muscles by using electromyograms (EMGs). In this technique, electrodes are placed on the skin overlaying a muscle. In humans, the electrodes are placed under the chin because muscles in this area demonstrate very dramatic changes during the various stages of sleep.

In practice, EEGs, EOGs, and EMGs are recorded simultaneously on continuously moving chart paper or digitized by a computer and displayed on a highresolution monitor. This allows the relationships among the three measurements to be seen immediately. The patterns of activity in these three systems provide the basis for classifying the different types of sleep.



Fig2.1: Placement of electrodes to determine EEG, EOG, and EMG.

Studying these events has led to the identification of two basic stages, or states, of sleep: non rapid eye movement (NREM) and rapid eye movement (REM).

Sleep is a highly organized sequence of events that follows a regular, cyclic program each night. Thus, the EEG, EMG, and EOG patterns change in predictable ways several times during a single sleep period. NREM sleep is divided into four stages according to the amplitude and frequency of brain wave activity.

- I NREM sleep: 4 stages (stage I, stage II, stage III, stage IV)
 - Stage I: sleep is also referred to as drowsiness or presleep and is the first or earliest stage of sleep. And usually consists of a combination of drop out of alpha activity and slow rolling eye movements.

The importance of normal sleep patterns is that they should not be mistaken for pathologic sharp waves. Several normal stage I patterns easily can be mistaken for epileptic sharp waves or spikes, including vertex sharp transients, POSTS, and even fragments of alpha rhythm as it drops out. Stage II: is the predominant sleep stage during a normal night's sleep. The distinct and principal EEG criterion to establish stage II sleep is the appearance of sleep spindles or K complexes. The presence of sleep spindles is necessary and sufficient to define stage II sleep. Another characteristic finding of stage II sleep is the appearance of K complexes, but since K complexes are typically associated with a spindle, spindles are the defining features of stage II sleep. Except for slow rolling eye movements, all patterns described under stage I persist in stage II sleep.

The stigmata of stage II sleep, spindles and K complexes, are usually easy to identify and are less subject to over interpretation or misinterpretation than the patterns of stage I sleep.

Stages III and IV of sleep are usually grouped together as "slow wave sleep" or "delta sleep." Slow wave sleep (SWS) is usually not seen during routine EEG, which is too brief a recording. However, it is seen during prolonged (>24 h) EEG monitoring.

II - REM sleep:

Rapid eye movement sleep, or REM sleep, accounts for 20–25% of total sleep time in most human adults. The criteria for REM sleep include rapid eye movements as well as a rapid low-voltage EEG. Most memorable dreaming occurs in this stage. At least in mammals, a descending muscular atonia is seen.

The duration of REM sleep increases progressively with each cycle and tends to predominate late in the sleep period into early morning. The occurrence of REM too soon after sleep onset, referred to as SOREMP, is considered pathological.



Fig2.2: Duration of sleep stages

In general, the EEG pattern of NREM sleep is slower, often more regular, and usually of higher voltage than that of wakefulness. As sleep gets deeper, the brain waves get slower and have greater amplitude. NREM Stage 1 is very light sleep; NREM Stage 2 has special brain waves called sleep spindles and K complexes; NREM Stages 3 and 4 show increasingly more high-voltage slow waves. In NREM Stage 4, it is extremely hard to be awakened by external stimuli. The muscle activity of NREM sleep is low, but the muscles retain their ability to function. Eye movements normally do not occur during NREM sleep, except for very slow eye movements, usually at the beginning. The body's general physiology during these stages is fairly similar to the wake state.

Sleep is a cyclical process. During sleep, people experience repeated cycles of NREM and REM sleep, beginning with an NREM phase. This cycle lasts approximately 90 to 110 minutes and is repeated four to six times per night. As the night progresses, however, the amount of deep NREM sleep decreases and the amount of REM sleep increase.



Fig2.3: A typical hypnogram from a young, healthy adult.

The chart in Fig2.3 is called a **hypnogram**. Hypnograms were developed to summarize the voluminous chart recordings of electrical activities (EEG, EOG, and EMG) collected during a night's sleep. Hypnograms provide a simple way to display information originally collected on many feet of chart paper or stored as a large file on a computer.

We can make several observations about the hypnogram in Fig2.3. First, the periods of NREM and REM sleep alternate during the night. Second, the deepest stages of NREM sleep occur in the first part of the night. Third, the episodes of REM sleep are longer as the night progresses. This hypnogram also indicates two periods during the night when the individual awakened (at about six and seven hours into the night).

It is useful to distinguish between sleep and the state induced during general anesthesia or seen in people who are in a coma.

2.2.2 Physiological changes during sleep

Table2 summarizes some basic physiological changes that occur in NREM and REM sleep.

Physiological					
Process	During NREM	During REM			
brain activity	decreases from wakefulness	increases in motor and sensory areas, while other areas are similar to NREM			
heart rate	slows from wakefulness	om wakefulness increases and varies compared with NREM			
blood pressure	decreases from wakefulness	increases (up to 30 percent) and varies from NREM			
blood flow to	does not change from wakefulness	increases by 50 to 200 percent			
brain	in most regions	from NREM, depending on brain region			
respiration	decreases from wakefulness	increases and varies from NREM, but may show brief stoppages (apnea); coughing suppressed			
airway resistance	increases from wakefulness	increases and varies from wakefulness			
body	is regulated at lower set point than	is not regulated; no shivering or			
temperature	wakefulness; shivering initiated at	sweating; temperature drifts			
	lower temperature than during	toward that of the local			
	wakefulness	environment			

Table 2.1: Comparison of Physiological Changes during NREM and REM sleep [7]

sexual arousal	occurs infrequently	increases from NREM (in both
		males and females)

2.2.3 Sleep and the brain

Sleep is actively generated in specific brain regions. These sites have been identified through studies involving electrical stimulation, damage to specific brain regions, or other techniques that identify sleep-inducing sites. The basal forebrain, including the hypothalamus, is an important region for controlling NREM sleep and may be the region keeping track of how long we have been awake and how large our sleep debt is.

The brainstem region known as the pons is critical for initiating REM sleep. As depicted in Fig2.4, during REM sleep, the pons sends signals to the visual nuclei of the thalamus and to the cerebral cortex (this region is responsible for most of our thought processes). The pons also sends signals to the spinal cord, causing the temporary paralysis that is characteristic of REM sleep. Other brain sites are also important in the sleep process. For example, the thalamus generates many of the brain rhythms in NREM sleep that we see as EEG patterns.



Fig2.4: Pathways of brain activity during REM sleep

2.2.4 Sleep Patterns:

Sleep patterns change during an individual's life. In fact, age affects sleep more than any other natural factor. One of the most prominent age-related changes in sleep is a reduction in the time spent in the deepest stages of NREM (Stages 3 and 4) from childhood through adulthood.

In fact, this change is prominent during adolescence, when about 40 percent of this activity is lost and replaced by Stage 2 NREM sleep. In addition to these changes, the percentage of time spent in REM sleep also changes during development.

Although most humans maintain REM sleep throughout life, brain disorders like Alzheimer's and Parkinson's are characterized by decreasing amounts of REM sleep as the diseases progress. Also, elderly individuals exhibit more variation in the duration and quality of sleep than do younger adults. Elderly people may also exhibit increased sleep fragmentation (arousals from sleep that occur as either short or more extended awakenings). The following table provides on average the amount of sleep a person needs according to their age.

Age	Total Sleep Needed	Additional Notes		
1-4 Weeks	15-16 Hours	Newborns are developing their internal biological clocks		
1-4 Months	14-15 Hours	Regular sleeping patterns begin and longer night sleeping		
4-12 Months	14-15 Hours	Important to establish regular sleeping patterns at this time		
1-3 Years	12-14 Hours	Naps remain important to sleep health		
3-6 Years	10-12 Hours	Naps will become shorter		
7-12 Years	10-11 Hours	Bedtime gets later		
12-18 Years	8-9 Hours	Teens may need more sleep		
Adults	7-8 Hours	Times will greatly vary		
Pregnant	8+	More sleep and naps may be needed		

Table2.2: Sleep Chart by Age [3]

2.2.5 Sleep Disorders:

Problems with sleep can be due to lifestyle choices and can result in problem sleepiness, which is, feeling sleepy at inappropriate times. Environmental noise, temperature changes, changes in sleeping surroundings, and other factors may affect our ability to get sufficient restful sleep. Short-term problem sleepiness may be corrected by getting additional sleep to overcome the sleep deficit. In other cases, problem sleepiness may indicate a sleep disorder requiring medical intervention.

Insomnia, the most prevalent sleep disorder, it is characterized by an inability to fall asleep and/or by waking up during the night and having difficulty going back to sleep

2.2.6 Insomnia:

Insomnia is a sleep disorder that is characterized by difficulty falling and/or staying asleep. People with insomnia have one or more of the following symptoms:

- Difficulty falling asleep
- Waking up often during the night and having trouble going back to sleep
- Waking up too early in the morning
- Feeling tired upon waking

There are two types of insomnia:

- 1- Primary insomnia.
- 2- Secondary insomnia.

• Primary insomnia:

Means that a person is having sleep problems that are not directly associated with any other health condition or problem.

• Secondary insomnia:

Means that a person is having sleep problems because of something else, such as a health condition; pain; medication they are taking; or a substance they are using (like alcohol).

Insomnia also varies in how long it lasts and how often it occurs. It can be shortterm (acute insomnia) or can last a long time (chronic insomnia). It can also come and go, with periods of time when a person has no sleep problems. Acute insomnia can last from one night to a few weeks. Insomnia is called chronic when a person has insomnia at least three nights a week for a month or longer.

According to that insomnia classified as:

- 1. **Transient insomnia** lasts for less than a week. It can be caused by another disorder, by changes in the sleep environment, by the timing of sleep, severe depression, or by stress.
- 2. Acute insomnia is the inability to consistently sleep well for a period of less than a month.
- 3. **Chronic insomnia** lasts for longer than a month. It can be caused by another disorder, or it can be a primary disorder. Its effects can vary according to its causes. They might include muscular fatigue, hallucinations, and/or mental fatigue. Some people that live with this disorder see things as if they are happening in slow motion, wherein moving objects seem to blend together. Can cause double vision.

Causes of Insomnia:

- Significant life stress
- Illness.
- Emotional or physical discomfort.

- Environmental factors like noise, light, or extreme temperatures (hot or cold) that interfere with sleep.
- Some medications (for example those used to treat colds, allergies, depression, and asthma) may interfere with sleep.

Causes of chronic insomnia include:

- Depression and/or anxiety
- Chronic stress.
- Pain or discomfort at night.

Symptoms of Insomnia:

- Sleepiness during the day.
- General tiredness.
- Irritability.
- Problems with concentration or memory.

Treatment for Insomnia:

- 4 Often can be prevented or cured by practicing good sleep habits.
- can use sleeping pills for a limited time (If the insomnia makes it hard to function during the day because sleepy and tired)
- Short-acting drugs can help avoid effects such as drowsiness the following day.
- Avoid using over-the-counter sleeping pills for insomnia since they may have undesired side effects and tend to lose their effectiveness over time.
- Try to go to sleep at the same time each night and get up at the same time each morning.
- Try not to take naps during the day because naps may make you less sleepy at night.
- Avoid caffeine, nicotine, and alcohol late in the day.

- Get regular exercise.
- **W** Don't eat a heavy meal late in the day.
- Make your bedroom comfortable , (quiet, no light , no sound ,)
- Follow a routine to help you relax before sleep. Read a book, listen to music, or take a bath.

2. 3 EEG (Electroencephalograph):

Electroencephalography (EEG): s the recording of electrical activity along the scalp. EEG measures voltage fluctuations resulting from ionic current flows within the neurons of the brain.

2.3.1 Different types of normal brain waves:

EEG wave groups:

- BETA. The electrical activity of the brain is varying within the range of 14 26 times per second (or Hz). A different name has been given to frequencies above 26 Hz but it is more usual to refer to these as fast beta waves. Beta is the usual waking rhythm of the brain associated with active thinking, active attention, focus on the outside world or solving concrete problems.
- 2. ALPHA. The rate of change lies between 8 and 13 Hz. Alpha waves have been thought to indicate both a relaxed awareness and also inattention. A receptive mind.

Alpha is the most prominent rhythm in the whole realm of brain activity and possibly covers a greater range than has been previously accepted. You can regularly see a peak in the beta range as high as 20 Hz, which has the characteristics of an alpha state rather than a beta, and the setting in which such a response appears also leads to the same conclusion. Again, we very often see a response at 75 Hz which appears in an 'alpha' setting. Most subjects produce some alpha with the eyes closed and this is why it has been claimed that it is nothing but a waiting or scanning pattern produced by the visual centers of the brain. It is reduced or eliminated by opening the eyes, by hearing unfamiliar sounds, by anxiety or mental concentration. Albert Einstein could solve complex mathematical problems while remaining in the alpha state, though our

work suggests that other frequencies, beta and theta would also have been present. Alpha alone seems to indicate an empty mind rather than a relaxed one, a mindless state rather than a passive one, and requires the presence of other frequencies, beta and theta before the usual description of alpha becomes true. Alpha, per se, is not associated with inwardly directed attention, relaxed awareness, or feelings of well being. In my project I'm primarily interested in learning to produce an alpha rhythm (despite the immense amount that has been written about it) rather what Γ m interested in experiencing is the particular calm detached state which happens to be accompanied by the alpha rhythm. Training to produce alpha on a biofeedback machine might therefore produce alpha without the sidebands beta and theta and therefore be experienced as a mindless and rather boring state.

- 3. THETA. Theta waves lie within the range of 4 to 7 Hz. Theta appears as consciousness slips toward drowsiness. Theta has been associated with access to unconscious material, creative inspiration and deep meditation. Theta is usually accompanied by other frequencies and seems rather to be related to level of arousal. We know that healers and experienced mediators have an alpha which gradually lowers in frequency over long periods of time. The large dominant peak of the 10 to 20 year mediator will almost certainly be found to be around 7 Hz in the so called theta band.
- 4. DELTA. Delta waves lie within the range of 1/2 to 4 Hz. Delta waves are primarily associated with deep sleep, and in the waking state, were thought to indicate physical defects in the brain.

It is very easy to confuse artifact signals caused by the large muscles of the neck and jaw with the genuine delta response. This is because the muscles are near the surface of the skin and produce large signals whereas the signal which is of interest originates deep in the brain and is severely attenuated in passing through the skull. Nevertheless, with an instant analysis EEG, it is very easy to see when the response is caused by excessive movement.

An EEG records patterns of brain activity. Among the basic waveforms are the alpha, beta, theta, and delta rhythms.
2.3.2 Important Points:

- 1. Sleep spindles and K complexes occur in stage II of NREM sleep.
- 2. Sleep spindles are short spindle shaped bursts of alpha waves that occur periodically in NREM sleep.
- 3. Frequency decreases and amplitude increases as we proceed from alpha to delta, the only exception is beta (highest frequency).

2.3.3 Relation with sleep:

Stage 0 -alpha- close eyes beta-open eyes stage 1 -alpha +theta stage 2- theta waves spindles k complexes stage 3- delta theta and spindle stage 4-delta REM sleep-all frequency of waves

2.4Geomagnetic field:

The Earth's magnetic field is generated in the fluid outer core by a self-exciting dynamo process. Electrical currents flowing in the slowly moving molten iron generate the magnetic field. In addition to sources in the Earth's core the magnetic field observable at the Earth's surface has sources in the crust and in the ionosphere and magnetosphere. The geomagnetic field varies on a range of scales and a description of these variations is now made, in the order low frequency to high frequency variations, in both the space and time domains.

Although scientists do not understand all of the details, they know that motions of molten metals in the Earth's core generate our planet's magnetic field. Movement of molten iron and nickel generates electrical and magnetic fields that produce Earth's magnetism. The flows of these molten metals in Earth's outer core are not perfectly steady over time, so Earth's magnetic field changes over time as well.

Earth's magnetic field extends thousands of kilometers (miles) outward into space. The field forms a gigantic magnetic "bubble" in space around Earth. This magnetic bubble is called the magnetosphere. Earth's magnetosphere shields our planet from most particle radiation that flow our way from the Sun and other radiation sources in space. The magnetosphere is not actually a sphere; it is shaped more like a teardrop, with a long "tail" extending away from the Sun.

This geomagnetic field shields us from dangerous gamma rays from the universe and at the same time forms a vital basis of stimulation for important metabolic processes in every cell in our body.

CHAPTER 3

Project Design

- 3.1 system elements
- **3.2 Project objectives**
- 3.3 Project circuit
 - **3.3.1** How To Use The Circuit
 - 3.3.2 Operation Of Circuit

3.1 System elements:

• Counter , timer and reset :

To provide different time durations counter is needed, in my project I choose 4060 IC (14 ripple counter and oscillator)



Fig .3.1: counter section



Fig.3.2: oscillator section of 4060 IC

To determine the values of R1 and C, first we determine the smallest desired

duration to determine the suitable pin for out put \longrightarrow Q11

The oscillator's frequency determined according to formula T= desired period (sec) / (8.5 * 2^a) (a=11) T = 15*60 /8.5 (2048) = 51.7 * 10^{-3} sec

F=1 / T= 1/51.7* 10⁻³ = 19.342222Hz

 $R3 = 10M\Omega, R4 \text{ must be} << R3, R4 = 2.2M\Omega$ $f \text{ osc} \approx 1 / 2.3R1 \text{ C} \rightarrow \text{C} = 100 \text{ nF}$

 \checkmark Reset section:

Depends on pressing the push button P1 corresponding with charging and discharging of C1.

While P1 not pressed the capacitor C1 charges and the voltage at R2 = 0 which means the reset pin is inactive (reset pin is active high).

When P1 is pressed, pin 12 will be supplied with voltage and the IC will reset its operation

 $R1{=}1K\Omega \qquad \qquad C1={47}\mu F$

Reset time = 5R1C1 = 0.235 sec

• IC1:4060 14 stage ripple counter and oscillator.

Features of 4060:

- All active components on chip
- RC or crystal oscillator configuration
- Output capability: standard (except for RTC and CTC)
- ICC category: MSI
- Inverter:



Fig.3.3: inverter and mode selection

This section plays the role of inverting the timing signal with the selected duration since the next stage turned on when the input in one of its terminals is low.

SW2 acts as mode selection, when it's open IC2A terminals take the value from the counter, when SW2 is closed IC2A terminals takes just one clock pulse then the internal oscillator of the previous stage will disabled

Oscillator:

Oscillators are devices that are used to generate repetitive signals. They produce output signals without an input signal. There are two major types of electronic oscillators: harmonic oscillators and relaxation oscillators.

Harmonic oscillators produce sine wave outputs. Relaxation oscillators produce non-sine wave outputs.

In my project I used 4093 IC (quad 2 input Schmitt NAND gate) to generate two square waves 1.4Hz and 5Hz (the frequencies varies between theta and delta waves of EEG)



Fig.3.4: Oscillator circuit



$$f = \frac{1}{t_1 + t_2} = \frac{1}{RC \ \ell \ n \frac{(V_T^+) (V_{DD} - V_T^-)}{(V_T^-)(V_{DD} - V_T^+)}}$$

From data sheet:

Vt + = 6.2 volt

Vt- = 4.1 volt

Vdd = 9 volt

So to generate the required frequency we choose proper values of R and C

For 1.4Hz

Let $R=2.2M\Omega$ then the suitable C=330nF

Similarly to 5Hz wave

 $R{=}10\ M\Omega \qquad and \quad C{=}330nF$

• IC2: 4093 Quad 2 input Schmitt NAND gate

Features of 4093:

- wide supply voltage range

- noise immunity greater than 50%
- no limit in input rise and fall time

Status indicator:



Fig.3.5: indicator circuit

This circuit to give an indication for the device status, pin5 is attached to the internal oscillator pin of 4060IC (pin 9), and pin6 to pin11 of the same IC (square wave signal with frequency 1.4Hz).

During driving the coil the LED will flash quickly, after the time duration is over the LED turned off.

Driving the coil:

Any electrical coil that is charged will produce an associated electromagnetic field. The higher the current, the stronger the electric field at a given distance from the wire.



Fig.3.6: coil driver circuit

A PNP transistor acts as switch that allow the two square wave signals after they converted into 60µs pulses to pass through the coil alternatively by means of D3.

D5 and D4 allow the current to pass in one direction so they prevent the transistor from the reversed currents

Features of BC327:

- High current (max. 500 mA)
- Low voltage (max. 45 V).

3.2 Project Objectives:

- 1) to study the physiology of sleep and brain waves (EEG)
- 2) be familiar with geomagnetic fields and how to generate it

 design and implement a device for generating the desired field with several durations and multi modes of operation

3.3 Project circuit:



Fig.3.7 Circuit diagram of the project

3.3.1 How To Use The Circuit

- *№* Select a timing option by means of the switch SW1.
- A Select "Stop" or "Alternate" mode operation by means of SW2.
- With SW2 closed (Stop mode operation) the electromagnetic radiation stops after the pre-set time is elapsed.
- With SW2 opened (Alternate mode operation) the device operates for the pre-set time, then pauses for the same amount of time: this cycle repeats indefinitely.
- *I* Place the unit under the pillow and enjoy sleeping.
- *№* To reset a cycle press P1 push button.

3.3.2 Operation Of Circuit

IC2C and IC2D generate two square waves at about 1.4Hz and 5 Hz respectively.

- These wave-forms are converted into 60µS pulses at the same frequencies by means of C5 & C6 and mixed at Q1 Base.
- This transistor drives the Radiator coil with a scalar series of pulses of 60µS length and 9V amplitude.
- *№* IC1, IC2A & IC2B form the timer section.
- № C1 & R2 provide auto-reset of IC1 at switch-on.
- The internal oscillator of IC1 drives the 14 stage ripple counter and, after about 15 minutes, output pin 1 goes high. Pin 3 of IC2A goes low and stops IC2C & IC2D oscillation.
- If SW2 is left open (Alternate mode operation), after 15 minutes pin 1 of IC1 goes low, pin 3 of IC2A goes high and oscillators are enabled again.
- If SW2 is closed (Stop mode operation), the first time output pin 1 of IC1 goes high, the internal oscillator of the IC is disabled by means of D1. Therefore the circuit remains off until a reset pulse is applied to pin 12 by means of P1 or when the whole device is switched-off and then restarted.
- The same thing occurs when SW1 is switched on 30 or 60 minutes positions, obviously changing time length.
- IC2B drives pilot LED D2 which operates in the following three modes:
 - Flashes quickly and almost randomly when the Radiator coil is driven
 - Flashes somewhat slowly and regularly when the Radiator coil is pausing during the Alternate mode operation
 - o Is off when the circuit auto-stops (Stop mode operation)

CHAPTER 4

Conclusion and Future Work

4.1 Conclusion & Results4.2 Future Works

4.1 Conclusions & Results:

Knowledge and practical experience were gained by developing this project. This project generates type of geo-magnetic-fields and it helps the brain surrounded by an ideal environment for a sound sleep. This project helps in fighting insomnia. Apart from this it also supports relaxation, stress management and induces sleep easily.

Faced problems:

- In my project for on/off and time duration selection, rotary switch is needed but I couldn't find it so I substitute it with three ordinary switches.

k Results:

After the construction of the device, for measuring the produced magnetic field I measure the current and then made my calculations.

The produced current is an alternating current, the resulted values from my device was 0.12mA - 0.16mA

 $B = \mu * I * L*N / 4pi * R^{2}$ Let R= 15cm N=300 turn L= 2pi*r*N $B = 4pi * 10^{-7} * 0.12*2pi*0.1*10^{-3}*300*300 / (4pi * (15*10^{-2})^{2})$ = 30 ntesla (within the range of Geomagnetic field)

 $B = 4pi *10^{-7} *0.16*2pi*0.1*10^{-3}*300*300 / (4pi * (15*10^{-2})^{2})$ = 40 ntesla (within the range of Geomagnetic field)

4.2 Future Work:

4.2.1 Magnetic energy Therapy:

The inducing of certain specifically pulsed magnetic energy fields into body tissue causes bioelectric current activity which may assist in the normalizing of electron flow within and between cells in the body. This may help in the temporary relief of pain and also in the repair damaged tissues.

Using extremely-ultra-low frequencies of 0.5 to 18Hz with specially shaped multi-rhythm bio-waveforms of oscillating magnetic energy fields,

The magnetic energy field frequencies must produced within the range of predominant brain frequencies of humans and animals. These are very different to the potentially damaging very high frequencies and waveforms of electro-magnetic radiation fields in the environment.

The explosion of use of magnets is now moving toward a new trend... the introduction of pulsed magnetic fields. Gentle, and easy to use, the cutting-edge concept of pulsed magnetic fields imitates the low magnetic fields that occur naturally in our bodies.

REFERENCES

[1] Rajeev Bansal, Engineering electromagnetic: application, 2009

[2] Introduction to biomedical equipment technology, fourth edition, Joseph J.Curr & John M.Brown.

RESEARCHS AND PAPERS:

[3] University of California and Sleep Research Society. Basics of sleep behavior. 1997. Retrieved July 17, 2001

[4] National Heart, Lung, and Blood Institute. Insomnia. Bethesda, MD: NHLBI;1995. (NIH Pub. No. 95-3801)

[5] Rechtschaffen, A.1998. Current perspectives on the function of sleep. Perspectives in Biological Medicine,

[6]Strohl, K.P., Haponik, E.E., Sateia, M.J., Veasey, S., Chervin, R.D., Zee, P., and Papp, K. 2000. The need for a knowledge system in sleep and chronobiology. Academic Medicine.

[7] Kohyama J. Sleep as a window on the developing brain. Current Problems in Pediatrics.

[8] Study on the influence of simulative EEG modulation magnetic field on the discharge of median raphe nuclei [Article in Chinese]

[9] Sleep. 1996 May; Effects of low energy emission therapy in chronic psycho physiological insomnia. Pasche B, Erman M, Hayduk R, Mitler MM, Reite M, Higgs L, Kuster N, Rossel C, Dafni U, Amato D, Barbault A, Lebet JP. Symtonic USA, Inc., New York, New York 10162, USA.

WEBSITES:

[10] www.redcircuits.com

[11]http://healingscience.bioenergeticspectrum.com/healingscienceframe.html?p ulsedmagnetictherapy.html

[12] http://www.alpha-

stim.lv/box/files/Pdf_dokumenti/Zinatniskie_petijumi/giluladepression.pdf

[12] www.wikipedia.com

[13] http://www.wisconsinengineer.com/articles/14

Appendix A

DATASHEETS

- 1. BC327
- 2. 4060 IC
- 3. 4093 IC

INTEGRATED CIRCUITS



Product specification File under Integrated Circuits, IC06 December 1990



74HC/HCT4060

FEATURES

- All active components on chip
- RC or crystal oscillator configuration
- Output capability: standard (except for R_{TC} and C_{TC})
- I_{CC} category: MSI

GENERAL DESCRIPTION

The 74HC/HCT4060 are high-speed Si-gate CMOS devices and are pin compatible with "4060" of the "4000B" series. They are specified in compliance with JEDEC standard no. 7A.

The 74HC/HCT4060 are 14-stage ripple-carry counter/dividers and oscillators with three oscillator

terminals (RS, R_{TC} and C_{TC}), ten buffered outputs (Q_3 to Q_9 and Q_{11} to Q_{13}) and an overriding asynchronous master reset (MR).

The oscillator configuration allows design of either RC or crystal oscillator circuits. The oscillator may be replaced by an external clock signal at input RS. In this case keep the other oscillator pins (R_{TC} and C_{TC}) floating.

The counter advances on the negative-going transition of RS. A HIGH level on MR resets the counter (Q_3 to Q_9 and Q_{11} to $Q_{13} = LOW$), independent of other input conditions.

In the HCT version, the MR input is TTL compatible, but the RS input has CMOS input switching levels and can be driven by a TTL output by using a pull-up resistor to V_{CC} .

QUICK REFERENCE DATA

GND = 0 V; T_{amb} = 25 °C; t_r = t_f = 6 ns

SYMBOL		CONDITIONS	TYP			
STWIDUL	FARAMETER	CONDITIONS	нс	нст		
t _{PHL} / t _{PLH}	propagation delay	C _L = 15 pF; V _{CC} = 5 V				
	RS to Q ₃		31	31	ns	
	Q _n to Q _{n+1}		6	6	ns	
t _{PHL}	MR to Q _n		17	18	ns	
f _{max}	maximum clock frequency		87	88	MHz	
CI	input capacitance		3.5	3.5	pF	
C _{PD}	power dissipation capacitance per package	notes 1, 2 and 3	40	40	pF	

Notes

1. C_{PD} is used to determine the dynamic power dissipation (P_D in μW):

 $P_D = C_{PD} \times V_{CC}^2 \times f_i + \sum (C_L \times V_{CC}^2 \times f_o)$ where:

 $f_i = input frequency in MHz$

 $f_o = output frequency in MHz$

 $\sum (C_L \times V_{CC}^2 \times f_0) = \text{sum of outputs}$

 C_L = output load capacitance in pF

V_{CC} = supply voltage in V

- 2. For HC the condition is $V_I = GND$ to V_{CC} For HCT the condition is $V_I = GND$ to $V_{CC} - 1.5$ V
- 3. For formula on dynamic power dissipation see next pages.

ORDERING INFORMATION

See "74HC/HCT/HCU/HCMOS Logic Package Information".

PIN DESCRIPTION

PIN NO.	SYMBOL	NAME AND FUNCTION
1, 2, 3	Q ₁₁ to Q ₁₃	counter outputs
7, 5, 4, 6, 14, 13, 15	Q ₃ to Q ₉	counter outputs
8	GND	ground (0 V)
9	C _{TC}	external capacitor connection
10	R _{TC}	external resistor connection
11	RS	clock input/oscillator pin
12	MR	master reset
16	V _{CC}	positive supply voltage



74HC/HCT4060

74HC/HCT4060

Product specification

DYNAMIC POWER DISSIPATION FOR 74HC

PARAMETER	V _{CC} (V)	TYPICAL FORMULA FOR P_D (μ W) (note 1)
total dynamic power	2.0	$C_{PD} \times f_{osc} \times V_{CC}^2 + \sum (C_L \times V_{CC}^2 \times f_o) + 2C_t \times V_{CC}^2 \times f_{osc} + 60 \times V_{CC}$
dissipation when using the	4.5	$C_{PD} \times f_{osc} \times V_{CC}^2 + \sum (C_L \times V_{CC}^2 \times f_o) + 2C_t \times V_{CC}^2 \times f_{osc} + 1750 \times V_{CC}$
on-chip oscillator (P _D)	6.0	$C_{PD} \times f_{osc} \times V_{CC}^2 + \Sigma \left(C_L \times V_{CC}^2 \times f_o \right) + 2C_t \times V_{CC}^2 \times f_{osc} + 3\ 800 \times V_{CC}$

Note

1. GND = 0 V; $T_{amb} = 25 \ ^{\circ}C$

DYNAMIC POWER DISSIPATION FOR 74HCT

PARAMETER	V _{CC} (V)	TYPICAL FORMULA FOR $P_D(\mu W)$ (note 1)
total dynamic power dissipation when using the on-chip oscillator (P _D)	4.5	$C_{PD} \times f_{osc} \times V_{CC}^2 + \Sigma \left(C_L \times V_{CC}^2 \times f_o \right) + 2C_t \times V_{CC}^2 \times f_{osc} + 1.750 \times V_{CC}$

Notes

- 1. GND = 0 V; $T_{amb} = 25 \degree C$
- 2. Where: f_0 = output frequency in MHz

fosc = oscillator frequency in MHz

- $\sum (C_L \times V_{CC}^2 \times f_o) = \text{sum of outputs}$
- C_L = output load capacitance in pF
- Ct = timing capacitance in pF
- V_{CC} = supply voltage in V



APPLICATIONS

- Control counters
- Timers
- Frequency dividers
- Time-delay circuits

74HC/HCT4060





74HC/HCT4060

DC CHARACTERISTICS FOR 74HC

Output capability: standard (except for R_{TC} and C_{TC}) I_{CC} category: MSI Voltages are referenced to GND (ground = 0 V)

					T _{amb} (°	°C)		TEST CONDITIONS				
SYM-					74H0	C						
BOL	PARAMETER	+25			-40 t	o +85	-40 1	to +125		V _{CC}	VI	UTHER
		min.	typ.	max.	min.	max.	min.	max.	1			
V _{IH}	HIGH level input voltage MR input	1.5 3.15 4.2	1.3 2.4 3.1		1.5 3.15 4.2		1.5 3.15 4.2		V	2.0 4.5 6.0		
V _{IL}	LOW level input voltage MR input		0.8 2.1 2.8	0.5 1.35 1.8		0.5 1.35 1.8		0.5 1.35 1.8	V	2.0 4.5 6.0		
V _{IH}	HIGH level input voltage RS input	1.7 3.6 4.8			1.7 3.6 4.8		1.7 3.6 4.8		V	2.0 4.5 6.0		
V _{IL}	LOW level input voltage RS input			0.3 0.9 1.2		0.3 0.9 1.2		0.3 0.9 1.2	V	2.0 4.5 6.0		
V _{OH}	HIGH level output voltage R _{TC} output	3.98 5.48			3.84 5.34		3.7 5.2		V	4.5 6.0	RS=GND and MR=GND	$-I_{O} = 2.6 \text{ mA}$ $-I_{O} = 3.3 \text{ mA}$
		3.98 5.48			3.84 5.34		3.7 5.2		V	4.5 6.0	RS=V _{CC} and MR=V _{CC}	$-I_{O} = 0.65 \text{ mA}$ $-I_{O} = 0.85 \text{ mA}$
		1.9 4.4 5.9	2.0 4.5 6.0		1.9 4.4 5.9		1.9 4.4 5.9		V	2.0 4.5 6.0	RS=GND and MR=GND	$-I_{O} = 20 \ \mu A$ $-I_{O} = 20 \ \mu A$ $-I_{O} = 20 \ \mu A$
		1.9 4.4 5.9	2.0 4.5 6.0		1.9 4.4 5.9		1.9 4.4 5.9		V	2.0 4.5 6.0	RS=V _{CC} and MR=V _{CC}	$-I_{O} = 20 \ \mu A$ $-I_{O} = 20 \ \mu A$ $-I_{O} = 20 \ \mu A$
V _{OH}	HIGH level output voltage C _{TC} output	3.98 5.48			3.84 5.34		3.7 5.2		V	4.5 6.0	RS=V _{IH} and MR=V _{IL}	$-I_{O} = 3.2 \text{ mA}$ $-I_{O} = 4.2 \text{ mA}$
V _{OH}	HIGH level output voltage except R _{TC} output	1.9 4.4 5.9	2.0 4.5 6.0		1.9 4.4 5.9		1.9 4.4 5.9		V	2.0 4.5 6.0	V _{IH} or V _{IL}	$-I_{O} = 20 \ \mu A$ $-I_{O} = 20 \ \mu A$ $-I_{O} = 20 \ \mu A$
V _{OH}	$\begin{array}{l} \text{HIGH level output voltage} \\ \text{except } \text{R}_{\text{TC}} \text{ and } \text{C}_{\text{TC}} \\ \text{outputs} \end{array}$	3.98 5.48			3.84 5.34		3.7 5.2		V	4.5 6.0	V _{IH} or V _{IL}	$-I_{O} = 4.0 \text{ mA}$ $-I_{O} = 5.2 \text{ mA}$
V _{OL}	LOW level output voltage R _{TC} output			0.26 0.26		0.33 0.33		0.4 0.4		4.5 6.0	RS=V _{CC} and MR=GND	$I_0 = 2.6 \text{ mA}$ $I_0 = 3.3 \text{ mA}$
			0 0 0	0.1 0.1 0.1		0.1 0.1 0.1		0.1 0.1 0.1	V	2.0 4.5 6.0	RS=V _{CC} and MR=GND	$I_{O} = 20 \ \mu A$ $I_{O} = 20 \ \mu A$ $I_{O} = 20 \ \mu A$

74HC/HCT4060

				-	T _{amb} (°	°C)		TEST CONDITIONS				
SYM-					74H0)			V			
BOL	PARAMETER	+25			-40 t	o +85	- 40 t	-40 to +125		V _{CC}	V I	UTHER
		min.	typ.	max.	min.	max.	min.	max.				
V _{OL}	LOW level output voltage C _{TC} output			0.26 0.26		0.33 0.33		0.4 0.4	V	4.5 6.0	RS=V _{IL} and MR=V _{IH}	I _O = 3.2 mA I _O = 4.2 mA
V _{OL}	LOW level output voltage except R _{TC} output		0 0 0	0.1 0.1 0.1		0.1 0.1 0.1		0.1 0.1 0.1	V	2.0 4.5 6.0	V _{IH} or V _{IL}	I _O = 20 μA I _O = 20 μA I _O = 20 μA
V _{OL}	LOW level output voltage except R_{TC} and C_{TC} outputs			0.26 0.26		0.33 0.33		0.4 0.4	V	4.5 6.0	V _{IH} or V _{IL}	I _O = 4.0 mA I _O = 5.2 mA
±lı	input leakage current			0.1		1.0		1.0	μA	6.0	V _{CC} or GND	
I _{CC}	quiescent supply current			8.0		80.0		160.0	μA	6.0	V _{CC} or GND	I _O = 0

74HC/HCT4060

AC CHARACTERISTICS FOR 74HC

 $GND = 0 V; t_r = t_f = 6 ns; C_L = 50 pF$

					T _{amb} (°		TES	TEST CONDITIONS				
SYMBOL					74HC	;					WAVEFORMS	
STIVIBUL	PARAMETER	+25			-40 t	to +85	-40 te	o +125			WAVEFORINS	
		min.	typ.	max.	min.	max.	min.	max.				
t _{PHL} / t _{PLH}	propagation delay RS to Q_3		99 36 29	300 60 51		375 75 64		450 90 77	ns	2.0 4.5 6.0	Fig.12	
t _{PHL} / t _{PLH}	propagation delay Q_n to Q_{n+1}		22 8 6	80 16 14		100 20 17		120 24 20	ns	2.0 4.5 6.0	Fig.14	
t _{PHL}	propagation delay MR to Q _n		55 20 16	175 35 30		220 44 37		265 53 45	ns	2.0 4.5 6.0	Fig.13	
t _{THL} / t _{TLH}	output transition time		19 7 6	75 15 13		95 19 16		110 22 19	ns	2.0 4.5 6.0	Fig.12	
t _W	clock pulse width RS; HIGH or LOW	80 16 14	17 6 5		100 20 17		120 24 20		ns	2.0 4.5 6.0	Fig.12	
t _W	master reset pulse width MR; HIGH	80 16 14	25 9 7		100 20 17		120 24 20		ns	2.0 4.5 6.0	Fig.13	
t _{rem}	removal time MR to RS	100 20 17	28 10 8		125 25 21		150 30 26		ns	2.0 4.5 6.0	Fig.13	
f _{max}	maximum clock pulse frequency	6.0 30 35	26 80 95		4.8 24 28		4.0 20 24		MHz	2.0 4.5 6.0	Fig.12	

DC CHARACTERISTICS FOR 74HCT

Output capability: standard (except for R_{TC} and C_{TC})

I_{CC} category: MSI

Voltages are referenced to GND (ground = 0 V)

		T _{amb} (°C)								TEST CONDITIONS				
					74HC	T			1			071155		
SYMBOL	PARAMETER	+25			-40 t	-40 to +85		o +125		V _{CC}	VI	OTHER		
		min.	typ.	max.	min.	max.	min.	max.		(-)				
VIH	HIGH level input voltage	2.0			2.0		2.0		V	4.5 to 5.5		note 2		
VIL	LOW level input voltage			0.8		0.8		0.8	V	4.5 to 5.5		note 2		
V _{OH}	HIGH level output voltage	3.98			3.84		3.7		V	4.5	RS=GND and MR=GND	-I _O = 2.6 mA		
	R _{TC} output	3.98			3.84		3.7		V	4.5	RS = V_{CC} and MR = V_{CC}	-I _O = 0.65 mA		
		4.4	4.5		4.4		4.4		V	4.5	RS=GND and MR=GND	-I _O = 20 μA		
		4.4	4.5		4.4		4.4		V	4.5	RS=V _{CC} and MR=V _{CC}	-I _O = 20 μA		
V _{OH}	HIGH level output voltage C_{TC} output	3.98			3.84		3.7		V	4.5	$RS = V_{IH}$ and $MR = V_{IL}$	-I _O = 3.2 mA		
V _{OH}	HIGH level output voltage except R_{TC} output	4.4	4.5		4.4		4.4		V	4.5	V _{IH} or V _{IL}	-I _O = 20 μA		
V _{OH}	HIGH level output voltage except R_{TC} and C_{TC} outputs	3.98			3.84		3.7		V	4.5	V _{IH} or V _{IL}	-l _O = 4.0 mA		
V _{OL}	LOW level output voltage			0.26		0.33		0.4	V	4.5	RS=V _{CC} and MR=GND	I _O = 2.6 mA		
	R _{TC} output		0	0.1		0.1		0.1	V	4.5	RS=V _{CC} and MR=GND	I _O = 20 μA		
V _{OL}	LOW level output voltage C _{TC} output			0.26		0.33		0.4	V	4.5	$RS = V_{IL}$ and $MR = V_{IH}$	I _O = 3.2 mA		
V _{OL}	LOW level output voltage except R _{TC} output		0	0.1		0.1		0.1	V	4.5	V _{IH} or V _{IL}	I _O = 20 μA		
V _{OL}	LOW level output voltage except R_{TC} and C_{TC} outputs			0.26		0.33		0.4	V	4.5	V _{IH} or V _{IL}	I _O = 4.0 mA		
±I	input leakage current			0.1		1.0		1.0	μA	5.5	V _{CC} or GND			
I _{CC}	quiescent supply current			8.0		80.0		160.0	μA	5.5	V _{CC} or GND	I _O = 0		
Δl _{CC}	additional quiescent supply current per input pin for unit load coefficient is 1 (note 1)		100	360		450		490	μA	4.5 to 5.5	V _{CC} – 2.1 V	other inputs at V_{CC} or GND; $I_{O} = 0$		

oscillator

Product specification

9

December 1990

Notes

- 1. The value of additional quiescent supply current (ΔI_{CC}) for a unit load of 1 is given here. To determine ΔI_{CC} per input, multiply this value by the unit load coefficient shown in the table below.
- 2. Only input MR (pin 12) has TTL input switching levels for the HCT versions.

INPUT	UNIT LOAD COEFFICIENT
MR	0.40

AC CHARACTERISTICS FOR 74HCT

 $GND = 0 V; t_r = t_f = 6 ns; C_L = 50 pF$

				-		TEST CONDITIONS					
SYMBOL					74HC			WAVEEODME			
STNIDUL	FARAMETER		+25			-40 to +85		-40 to +125		V _{CC}	WAVEFORMIS
		min.	typ.	max.	min.	max.	min.	max.			
t _{PHL} / t _{PLH}	propagation delay RS to Q_3		33	66		83		99	ns	4.5	Fig.12
t _{PHL} / t _{PLH}	propagation delay Q_n to Q_{n+1}		8	16		20		24	ns	4.5	Fig.14
t _{PHL}	propagation delay MR to Q _n		21	44		55		66	ns	4.5	Fig.13
t _{THL} / t _{TLH}	output transition time		7	15		19		22	ns	4.5	Fig.12
t _W	clock pulse width RS; HIGH or LOW	16	6		20		24		ns	4.5	Fig.12
t _W	master reset pulse width MR; HIGH	16	6		20		24		ns	4.5	Fig.13
t _{rem}	removal time MR to RS	26	13		33		39		ns	4.5	Fig.13
f _{max}	maximum clock pulse frequency	30	80		24		20		MHz	4.5	Fig.12

74HC/HCT4060

74HC/HCT4060



TIMING COMPONENT LIMITATIONS

The oscillator frequency is mainly determined by R_tC_t , provided $R2 \approx 2R_t$ and $R2C2 \ll R_tC_t$. The function of R2 is to minimize the influence of the forward voltage across the input protection diodes on the frequency. The stray capacitance C2 should be kept as small as possible. In consideration of accuracy, C_t must be larger than the inherent stray capacitance. R_t must be larger than the "ON" resistance in series with it, which typically is 280 Ω at V_{CC} = 2.0 V, 130 Ω at V_{CC} = 4.5 V and 100 Ω at V_{CC} = 6.0 V.

The recommended values for these components to maintain agreement with the typical oscillation formula are: $C_t > 50 \text{ pF}$, up to any practical value,

10 k Ω < R_t < 1 M Ω .

In order to avoid start-up problems, $R_t \ge 1 \ k\Omega$.

74HC/HCT4060



AC WAVEFORMS





PACKAGE OUTLINES

See "74HC/HCT/HCU/HCMOS Logic Package Outlines".



CD4093BM/CD4093BC Quad 2-Input NAND Schmitt Trigger

General Description

The CD4093B consists of four Schmitt-trigger circuits. Each circuit functions as a 2-input NAND gate with Schmitt-trigger action on both inputs. The gate switches at different points for positive and negative-going signals. The difference between the positive (V_T⁺) and the negative voltage (V_T⁻) is defined as hysteresis voltage (V_H).

All outputs have equal source and sink currents and conform to standard B-series output drive (see Static Electrical Characteristics).

Features

- Wide supply voltage range
- Schmitt-trigger on each input
- with no external components
- Noise immunity greater than 50%

Connection Diagram

Equal source and sink currents

- No limit on input rise and fall time
 Standard B-series output drive
- $\label{eq:constraint} \begin{array}{|c|c|c|} \blacksquare & \mbox{Hysteresis voltage (any input) } T_A &= 25^\circ C \\ \hline Typical & V_{DD} &= 5.0V & V_H &= 1.5V \\ V_{DD} &= 10V & V_H &= 2.2V \\ V_{DD} &= 15V & V_H &= 2.7V \end{array}$
 - Guaranteed

Applications

- Wave and pulse shapers
- High-noise-environment systems
- Monostable multivibrators
- Astable multivibrators
- NAND logic

3.0V to 15V



CD4093BM/CD4093BC Quad 2-Input NAND Schmitt Trigger

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February 1993

 $V_H = 0.1 V_{DD}$

 $\label{eq:spectral_$

DC Supply Voltage (V _{DD})	-0.5 to $+18$ V _{DC}
Input Voltage (V _{IN})	-0.5 to $V_{\mbox{DD}}$ $+0.5$ $V_{\mbox{DC}}$
Storage Temperature Range (T _S)	-65°C to +150°C
Power Dissipation (P _D)	
Dual-In-Line	700 mW
Small Outline	500 mW
Lead Temperature (T _L)	
(Soldering, 10 seconds)	260°C

Recommended Operating Conditions (Note 2)

COnditions (Note 2)	
DC Supply Voltage (V _{DD})	3 to 15 V _{DC}
Input Voltage (V _{IN})	0 to $V_{DD} V_{DC}$
Operating Temperature Range (T _A) CD4093BM CD4093BC	-55°C to +125°C -40°C to +85°C

DC Electrical Characteristics CD4093BM (Note 2)

Symbol	Parameter	Conditions	−55°C		+ 25°C			+ 125°C		Unite
Symbol		Conditions	Min	Max	Min	Тур	Max	Min	Max	
I _{DD}	Quiescent Device Current	$V_{DD} = 5V$ $V_{DD} = 10V$ $V_{DD} = 15V$		0.25 0.5 1.0			0.25 0.5 1.0		7.5 15.0 30.0	μΑ μΑ μΑ
V _{OL}	Low Level Output Voltage			0.05 0.05 0.05		0 0 0	0.05 0.05 0.05		0.05 0.05 0.05	V V V
V _{OH}	High Level Output Voltage		4.95 9.95 14.95		4.95 9.95 14.95	5 10 15		4.95 9.95 14.95		V V V
V _T -	Negative-Going Threshold Voltage (Any Input)	$\begin{split} I_{O} &< 1 \; \mu A \\ V_{DD} &= 5 V, V_{O} = 4.5 V \\ V_{DD} &= 10 V, V_{O} = 9 V \\ V_{DD} &= 15 V, V_{O} = 13.5 V \end{split}$	1.3 2.85 4.35	2.25 4.5 6.75	1.5 3.0 4.5	1.8 4.1 6.3	2.25 4.5 6.75	1.5 3.0 4.5	2.3 4.65 6.9	V V V
V _T +	Positive-Going Threshold Voltage (Any Input)	$\begin{split} I_{O} &< 1 \; \mu A \\ V_{DD} &= 5 V, V_{O} &= 0.5 V \\ V_{DD} &= 10 V, V_{O} &= 1 V \\ V_{DD} &= 15 V, V_{O} &= 1.5 V \end{split}$	2.75 5.5 8.25	3.65 7.15 10.65	2.75 5.5 8.25	3.3 6.2 9.0	3.5 7.0 10.5	2.65 5.35 8.1	3.5 7.0 10.5	V V V
V _H	Hysteresis (V _T ⁺ - V _T ⁻) (Any Input)	$V_{DD} = 5V$ $V_{DD} = 10V$ $V_{DD} = 15V$	0.5 1.0 1.5	2.35 4.30 6.30	0.5 1.0 1.5	1.5 2.2 2.7	2.0 4.0 6.0	0.35 0.70 1.20	2.0 4.0 6.0	V V V
I _{OL}	Low Level Output Current (Note 3)		0.64 1.6 4.2		0.51 1.3 3.4	0.88 2.25 8.8		0.36 0.9 2.4		mA mA mA
I _{OH}	High Level Output Current (Note 3)		-0.64 -1.6 -4.2		0.51 -1.3 -3.4	-0.88 -2.25 -8.8		-0.36 -0.9 -2.4		mA mA mA
I _{IN}	Input Current	$\begin{array}{l} V_{DD}=15V, V_{IN}=0V\\ V_{DD}=15V, V_{IN}=15V \end{array}$		-0.1 0.1		-10 ⁻⁵ 10 ⁻⁵	-0.1 0.1		-1.0 1.0	μΑ μΑ

Note 1: "Absolute Maximum Ratings" are those values beyond which the safety of the device cannot be guaranteed; they are not meant to imply that the devices should be operated at these limits. The table of "Recommended Operating Conditions" and "Electrical Characteristics" provides conditions for actual device operation.

Note 2: $V_{SS}\,=\,$ 0V unless otherwise specified.

Note 3: $I_{\mbox{OH}}$ and $I_{\mbox{OL}}$ are tested one output at a time.

Symbol	Paramotor	Conditions		-40°C		+ 25°C			+ 85°C		11	
Symbol	Parameter			Min	Max	Min	Тур	Max	Min	Max		
I _{DD}	Quiescent Device	$V_{DD} = 5V$			1.0			1.0		7.5	μA	
	Current	$V_{DD} = 10V$			2.0			2.0		15.0	μA	
N/			1		4.0			4.0		30.0	μΑ	
VOL	Output Voltage	$V_{DD} = 5V$	ΓμΑ		0.05		0	0.05		0.05	v	
		$V_{DD} = 10V$			0.05		0	0.05		0.05	V	
		$V_{DD} = 15V$			0.05		0	0.05		0.05	V	
V _{OH}	High Level	$ V_{IN} = V_{SS}, I_0 <$	1 μΑ	4.05		4.05	5		4.05		V	
	Oulput voltage	ν _{DD} = 3ν ν _{DD} = 10ν		4.95 9.95		4.95 9.95	10		4.95 9.95		v	
		$V_{DD} = 15V$		14.95		14.95	15		14.95		V	
V _T -	Negative-Going Threshold	$ I_0 < 1 \ \mu A$										
	Voltage (Any Input)	$V_{DD} = 5V, V_O = 4$	4.5V	1.3	2.25	1.5	1.8	2.25	1.5	2.3	V	
		$V_{DD} = 10V, V_{O} = 15V, V_{O} = 15V$	9V 13.5V	2.85	4.5 6.75	3.0 4.5	4.1 6.3	4.5 6.75	3.0 4.5	4.65		
V _T +	Positive-Going Threshold	$ _{O} < 1 \mu A$	10.01	1.00	0.10	1.0	0.0	0.70	1.0	0.0		
۷I	Voltage (Any Input)	$V_{DD} = 5V, V_{O} = 0$).5V	2.75	3.6	2.75	3.3	3.5	2.65	3.5	v	
		$V_{DD} = 10V, V_{O} =$	1V	5.5	7.15	5.5	6.2	7.0	5.35	7.0	V	
		$V_{DD} = 15V, V_{O} =$	1.5V	8.25	10.65	8.25	9.0	10.5	8.1	10.5	V	
V _H	Hysteresis ($V_T^+ - V_T^-$)	$V_{DD} = 5V$		0.5	2.35	0.5	1.5	2.0	0.35	2.0	V	
	(Any Input)	$V_{DD} = 10V$ $V_{DD} = 15V$		1.0 1.5	4.3	1.0 1.5	2.2	4.0	0.70	4.0 6.0		
	Low Level Output											
'OL	Current (Note 3)	$V_{DD} = 5V, V_O = 0$).4V	0.52		0.44	0.88		0.36		mA	
		$V_{DD} = 10V, V_O =$	0.5V	1.3		1.1	2.25		0.9		mA	
		$V_{DD} = 15V, V_{O} =$	1.5V	3.6		3.0	8.8		2.4		mA	
ЮН	High Level Output	$V_{IN} = V_{SS}$	1.61/	_0.52		0.44	-0.88		_0.36		mΔ	
	ourient (Note 5)	$V_{DD} = 30, V_{O} = 10$	9.5V	-1.3		-1.1	-2.25		-0.9		mA	
		$V_{DD} = 15V, V_{O} =$	13.5V	-3.6		-3.0	-8.8		-2.4		mA	
I _{IN}	Input Current	$V_{DD} = 15V, V_{IN} =$	0V		-0.3		-10^{-5}	-0.3		-1.0	μA	
		$V_{DD} = 15V, V_{IN} =$	15V		0.3		10 ⁻⁵	0.3		1.0	μΑ	
	Electrical Charact	orietice*										
$T_A = 2$	25° C, C _L = 50 pF, R _L = 20	$0k$, Input t_r , $t_f = 20$	ns, unle	ess other	wise sp	ecified						
Symbol Para		neter Condition		nditions		Min	σγΤ		Max	Units		
tou.	TRUH Propagation De	Propagation Delay Time		n = 5V		300		450		ns		
"FIL			$V_{DD} = 10V$				120		210	0		
				$V_{DD} = 15V$		80			160		ns	
t _{THL} ,	t _{TLH} Transition Time	H Transition Time V _D		$V_{DD} = 5V$			90		145		ns	
				D = 10V			50		75 60		ns	
	leave Orace "					40			7.5			
	Input Capacitar		(A)	Any Input)			5.0		1.5	p⊢		
C _{PD}	Power Dissipat	ion Capacitance	P (P	er Gate)			24				p⊢	

*AC Parameters are guaranteed by DC correlated testing.

Note 2: $V_{SS}\,=\,$ 0V unless otherwise specified.

Note 3: $I_{\mbox{OH}}$ and $I_{\mbox{OL}}$ are tested one output at a time.









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DISCRETE SEMICONDUCTORS



Product specification Supersedes data of 1997 Mar 10 1999 Apr 15



FEATURES

- High current (max. 500 mA)
- Low voltage (max. 45 V).

APPLICATIONS

• General purpose switching and amplification, e.g. driver and output stages of audio amplifiers.

DESCRIPTION

PNP transistor in a TO-92; SOT54 plastic package. NPN complement: BC337.

PINNING

PIN	DESCRIPTION	
1	emitter	
2	base	
3	collector	



Fig.1 Simplified outline (TO-92; SOT54) and symbol.

LIMITING VALUES

In accordance with the Absolute Maximum Rating System (IEC 134).

SYMBOL	PARAMETER	CONDITIONS	MIN.	MAX.	UNIT
V _{CBO}	collector-base voltage	open emitter	-	-50	V
V _{CEO}	collector-emitter voltage	open base	-	-45	V
V _{EBO}	emitter-base voltage	open collector	-	-5	V
I _C	collector current (DC)		-	-500	mA
I _{CM}	peak collector current		-	-1	A
I _{BM}	peak base current		-	-200	mA
P _{tot}	total power dissipation	$T_{amb} \le 25 \ ^{\circ}C$; note 1	_	625	mW
T _{stg}	storage temperature		-65	+150	°C
Tj	junction temperature		_	150	°C
T _{amb}	operating ambient temperature		-65	+150	°C

Note

1. Transistor mounted on an FR4 printed-circuit board.

BC327

BC327

THERMAL CHARACTERISTICS

SYMBOL	PARAMETER	CONDITIONS	VALUE	UNIT
R _{th j-a}	thermal resistance from junction to ambient	note 1	0.2	K/mW

Note

1. Transistor mounted on an FR4 printed-circuit board.

CHARACTERISTICS

 $T_j = 25 \ ^{\circ}C$ unless otherwise specified.

SYMBOL	PARAMETER	CONDITIONS	MIN.	TYP.	MAX.	UNIT
I _{CBO}	collector cut-off current	$I_E = 0; V_{CB} = -20 V$	_	_	-100	nA
		$I_E = 0; V_{CB} = -20 V; T_j = 150 °C$	-	-	-5	μA
I _{EBO}	emitter cut-off current	$I_{C} = 0; V_{EB} = -5 V$	-	_	-100	nA
h _{FE}	DC current gain	$I_{C} = -100 \text{ mA}; V_{CE} = -1 \text{ V};$				
	BC327	see Figs 2, 3 and 4	100	-	600	
	BC327-16		100	-	250	
	BC327-25		160	-	400	
	BC327-40		250	-	600	
h _{FE}	DC current gain	$I_{\rm C} = -500 \text{ mA}; V_{\rm CE} = -1 \text{ V};$	40	-	-	
		see Figs 2, 3 and 4				
V _{CEsat}	collector-emitter saturation voltage	$I_{\rm C} = -500 \text{ mA}; I_{\rm B} = -50 \text{ mA}$	-	-	-700	mV
V_{BE}	base-emitter voltage	$I_{C} = -500 \text{ mA}; V_{CE} = -1 \text{ V}; \text{ note } 1$	_	_	-1.2	V
C _c	collector capacitance	$I_E = i_e = 0; V_{CB} = -10 V; f = 1 MHz$	-	10	-	pF
f _T	transition frequency	$I_{C} = -10 \text{ mA}; V_{CE} = -5 \text{ V};$ f = 100 MHz	80	—	_	MHz

Note

1. V_{BE} decreases by about –2 mV/K with increasing temperature.

BC327

PNP general purpose transistor





BC327

PNP general purpose transistor



PACKAGE OUTLINE



BC327

Product specification

BC327

DEFINITIONS

Data sheet status				
Objective specification	ive specification This data sheet contains target or goal specifications for product development.			
Preliminary specification	This data sheet contains preliminary data; supplementary data may be published later.			
Product specification	This data sheet contains final product specifications.			
Limiting values				
Limiting values given are in accordance with the Absolute Maximum Rating System (IEC 134). Stress above one or more of the limiting values may cause permanent damage to the device. These are stress ratings only and operation of the device at these or at any other conditions above those given in the Characteristics sections of the specification is not implied. Exposure to limiting values for extended periods may affect device reliability.				
Application information				

Where application information is given, it is advisory and does not form part of the specification.

LIFE SUPPORT APPLICATIONS

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